

1 **Effect of Dielectric Filter Discharge Plasma on the Inactivation of**

2 **Aerosolized Pathogens Associated with Edible Insects**

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ABSTRACT

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The objective of this study was to determine the optimal disinfection treatment conditions of dielectric filter discharge (DFD) plasma against aerosolized pathogens relevant to edible insect-rearing environments. *Bacillus thuringiensis*, *Serratia marcescens*, and *Escherichia coli* O157:H7 are representative pathogens that may occur in edible insect-rearing environments. This study employed a treatment scheme in which plasma was applied during nebulization to treat aerosolized pathogens, after collection to treat filter-attached pathogens, or sequentially to both (overall pathogens). Negligible or minimal bactericidal effects were observed when DFD plasma was applied to aerosolized or filter-attached pathogens for 2 min. However, continuous treatment of both for 2 min each (a total of 4 min) resulted in significant inactivation, and longer treatment times (10 min) for filter-attached pathogens further enhanced the bactericidal effect (2.6~3.4 Log CFU/cm² reduction). No bactericidal effect was observed during storage after DFD plasma was turned off. Consequently, the highest bactericidal effect was obtained when DFD plasma was applied to aerosolized pathogens for 2 min, followed by an additional 10 min of treatment with filter-attached pathogens. These results indicate the potential use of DFD plasma for disinfecting aerosolized pathogens in edible insect-rearing environments.

Keywords: aerosolized pathogens; bacterial inactivation; cold plasma; edible insect

INTRODUCTION

42

43 The global population is expected to reach 9.8 billion by 2050, resulting in over a 70% increase in the demand
44 for animal-based protein sources [1]. Edible insects rich in proteins, essential amino acids, and fatty acids are
45 emerging as promising alternatives to conventional meat [2]. Additionally, rearing edible insects is more eco-
46 friendly than livestock production because of their lower space and water requirements and greenhouse gas
47 emissions. Accordingly, the number of edible insect farms is increasing worldwide [2].

48 In most edible insect farms, larvae are raised in enclosed spaces with high larval densities to maximize space
49 efficiency [3]. However, this rearing process provides favorable conditions for pathogen proliferation and
50 transmission, resulting in disease outbreaks and decreased productivity [3]. Pathogenic bacteria, such as *Bacillus*
51 *thuringiensis* and *Serratia marcescens*, are lethal to Coleoptera and Lepidoptera, posing serious challenges during
52 insect rearing. *S. marcescens* is pathogenic in humans [4]. *B. thuringiensis* has enterotoxin genes similar to those
53 of *Bacillus cereus*, which may be associated with foodborne outbreaks [5]. Additionally, edible insects are reported
54 to carry Shiga toxin-producing *E. coli*, including several pathogenic strains such as *E. coli* O157:H7, some of
55 which cause foodborne illnesses [6]. Therefore, pathogenic bacteria that contaminate insect-rearing environments
56 must be inactivated to ensure efficient insect production, protect human health, and enhance microbial safety
57 during product consumption.

58 When living organisms, such as edible insects, are reared, pathogenic bacteria may not merely adhere to
59 surfaces but can also exist in the air [7, 8]. Bacteria can be present in the air attached to airborne particles such as
60 aerosols [9]. These aerosolized bacteria can be carried upward by convective air currents, and given their small
61 size, they can persist in the air for a long time [9]. Bacteria can travel several meters from their origin, reach
62 various surfaces, and pose the risk of secondary transmission [10]. To effectively prevent indoor transmission in
63 edible insect farms, it is necessary to use an appropriate air disinfection system to inactivate pathogenic insect
64 aerosols.

65 Various methods can be used to disinfect the air. Among non-chemical methods, filtration is the most commonly
66 used. Various filters, such as high-efficiency particulate air (HEPA) and polypropylene melt-blown (PP) filters,
67 are used to filter air in masks, medical devices, and air purifiers [11, 12]. However, such filters only capture
68 aerosolized microorganisms on their surfaces without inactivating them, leading to the risk of secondary

69 transmission through ventilation systems [13]. Therefore, filtration methods must be used in combination with
70 other disinfection methods.

71 Plasma is an emerging technology capable of disinfecting air and inactivating microorganisms when combined
72 with various filters. Atmospheric plasma generates electromagnetic fields, UV photons, and reactive oxygen and
73 nitrogen species (RONS), which play key roles in microbicidal activity [10]. Previous studies have shown that a
74 plasma device coupled with a filter can remove and inactivate aerosolized microorganisms [14]. Baek et al. [10]
75 developed a dielectric filter discharge (DFD) plasma device in which plasma was coupled with a PP filter and
76 used to inactivate SARS-CoV-2 aerosols. However, most studies on plasma coupled with filter devices have
77 focused on viral inactivation, and although some studies targeting bacteria have been reported, no studies have
78 reported inactivation of pathogens that may occur during the rearing of edible insects. Additionally, it is necessary
79 not only to evaluate the bactericidal effect of the plasma coupled with a filter device but also to identify the most
80 effective processing conditions for bacterial inactivation.

81 The objective of this study was to evaluate optimal conditions for inactivating aerosolized pathogens related to
82 edible insects (*B. thuringiensis*, *S. marcescens*, and *E. coli* O157:H7) using DFD plasma in which surface
83 discharge occurs on a porous dielectric (air-passable) filter. The bactericidal effects were compared when
84 pathogens were treated in the aerosolized state, after being attached to the filter, under continuous treatment of
85 both states, and during storage time after plasma treatment.

86

87 **MATERIALS AND METHODS**

88 **DFD Plasma Source**

89 The DFD plasma source used in this study was identical to that described by Baek et al. [10]. The DFD plasma
90 generator was designed for air permeability. Both sides of 3 mm zirconium oxide beads were covered with
91 punched aluminum electrodes (0.5 mm thick, 2 mm punching hole diameter), forming a porous dielectric filter
92 barrier.

93

94 **Bacterial Strains and Microbial Preparation**

95 *B. thuringiensis* (KACC 12061) and *S. marcescens* (KACC 11961) were cultivated in a 25 mL nutrient broth
96 (MB cell, Seoul, Korea) at 30°C for 24 h, respectively. *E. coli* O157:H7 (NCCP 17169) was cultivated in a 25 mL

97 tryptic soy broth (MB cell, Seoul, Korea) at 37°C for 24 h. The cultures were washed as described by Yong et al.
98 [15]. Finally, microbial pellets were resuspended in 25 mL sterile saline with optical density (600 nm) adjusted to
99 0.5. Final viable cell densities of the pathogens were approximately 10^{7-8} CFU/mL, respectively. Each pathogen
100 suspension was prepared and aerosolized independently for all subsequent plasma treatments.

101

102 **Generating and Treating Aerosols with DFD Plasma**

103 The bacterial suspension was aerosolized using a nebulizer (HL100A; JOINMEDICAL, Seoul, Korea) to
104 generate aerosolized pathogens. The nebulizer was connected to a closed cylindrical chamber equipped with a
105 DFD plasma system (Fig. 1 (a)), as described by Baek et al. [10]. The pump was operated at 25 L/min during
106 nebulization and then turned off. Aerosolized pathogens were passed through the plasma zone under a sinusoidal
107 voltage of 1.24 kV at 8 kHz using ambient air at room temperature. Fig. 1 (b) shows voltage and current waveforms
108 of the DFD plasma generator, illustrating typical dielectric barrier discharge (DBD) behavior. Pathogens were
109 collected on a PP filter below the generator (99.95% efficiency for 0.3 μ m particles), which was UV-sterilized for
110 30 min on both sides before use. HEPA filters were installed at the air inlet and outlet to prevent the release of
111 pathogens. Control samples were prepared under identical conditions without plasma exposure.

112

113 **Experimental Design of DFD Plasma Treatment**

114 The experimental design of this study is illustrated in Fig. 2. In Experiment I, the bactericidal effects of DFD
115 plasma were evaluated against aerosolized and filter-attached pathogens, and this evaluation was further extended
116 to include continuous treatment with DFD plasma for both pathogen types (overall pathogens). For aerosolized
117 pathogen treatment, plasma was operated during nebulization so that airborne bacteria were treated with DFD
118 plasma for 2 min. For the filter-attached pathogen treatment, nebulization was performed without plasma
119 operation; aerosolized pathogens were collected on the PP filter, and the filter-attached pathogens were
120 subsequently treated with DFD plasma for 2 min. Thus, plasma exposure during nebulization targeted only
121 aerosolized pathogens, whereas plasma exposure after nebulization targeted only filter-attached pathogens. For
122 overall pathogen treatment, DFD plasma was applied for 2 min during nebulization and 2 min after nebulization
123 to assess its continuous inactivation effect on both aerosolized and filter-attached pathogens (total treatment time:
124 4 min).

125 In Experiment II, the bactericidal effect on overall pathogens with different storage times after DFD plasma
126 treatment was evaluated. DFD plasma was applied for 2 min during nebulization and for an additional 2 min after
127 nebulization to treat the overall pathogens, after which the plasma was turned off. To assess residual bactericidal
128 effect during storage after the plasma was turned off, the PP filter with attached pathogens was placed inside the
129 device for 0 and 1 min. As shown in Fig. 3 (b), it takes 1 min for the ozone concentration inside the device to
130 reach zero after the plasma is turned off; therefore, the maximum storage time was set to 1 min.

131 In Experiment III, DFD plasma was applied to aerosolized pathogens for 2 min, followed by additional
132 treatments for 2, 5, and 10 min on filter-attached pathogens to evaluate bactericidal effects.

133

134 **Microbial Analysis**

135 After plasma treatment, each PP filter was vortexed with 20 mL of sterile saline for 2 min. The resulting
136 suspension was serially diluted in saline. *B. thuringiensis* and *S. marcescens* were plated on nutrient agar, and *E.*
137 *coli* O157:H7 was plated on tryptic soy agar (MB cell, Seoul, Korea). Aliquots (0.1 mL) were spread onto plates
138 and incubated for 48 h at 30°C (*B. thuringiensis*, *S. marcescens*) or 37°C (*E. coli* O157:H7). The colony-forming
139 units (CFU/cm²) were calculated as density using the following formula:

$$140 \quad \text{Density} = \frac{\text{Avg. count}}{\text{Drop volume}} \times \text{Dilution} \times \text{Volume used to resuspend} \times \frac{1}{\text{Surface area}}$$

141 where Avg. count is the average of the raw data counts [CFU];

142 Drop volume is defined as the volume of the sample placed on the agar plate [mL]; Dilution is the 1/10^k,
143 where k is an integer for 10-fold dilutions [no units];

144 Volume used for resuspension was the liquid volume required to resuspend the PP filter [mL];

145 Surface area is the resuspended surface area of the PP filter [cm²].

146

147 **Optical Emission Spectroscopy and Ozone Concentration**

148 The optical emission spectrum of the DFD plasma was recorded using a spectrometer (Maya 2000 PRO, Ocean
149 Insight, Orlando, FL, USA) with an appropriate optical setup. The ozone concentration generated during plasma
150 operation was monitored using a UV ozone analyzer (UV-106L; 2 B Technologies, Broomfield, CO, USA) in
151 three stages: i) DFD plasma treatment of aerosolized pathogens, ii) DFD plasma treatment of filter-attached
152 pathogens, and iii) post-treatment storage time. All ozone concentration generated during plasma operation was

153 measured under conditions without nebulization of the bacterial suspension.

154

155 **Statistical Analysis**

156 All data represent the mean values of three replicates. Statistical analysis was performed using one-way
157 ANOVA in a completely randomized design with IBM SPSS software (v20.0; IBM SPSS Inc., Chicago, IL, USA).
158 Significant differences among treatments were determined using Duncan's multiple range test ($p < 0.05$).

159

160 **RESULTS AND DISCUSSION**

161 **Optical Emission Spectroscopy and Ozone Concentration**

162 Optical emission spectroscopy was used to identify the reactive species generated by DFD plasma. As shown
163 in Fig. 3 (a), the spectrum exhibited strong emission bands from molecular nitrogen (N_2) and its ionized form
164 (N_2^+). The intense emission at 300–400 nm corresponds to the second positive system ($C^3\Pi_u-B^3\Pi_g$) of N_2 ,
165 indicating excitation by energetic electrons, while the 380–470 nm region represents the first negative system
166 ($B^2\Sigma_u^+-X^2\Sigma_g^+$) of N_2^+ , reflecting plasma ionization. These results confirm that the DFD plasma operated in air
167 produced excited N_2^* and N_2^+ species, which serve as precursors for downstream RONS, such as O_3 , $OH\cdot$, and
168 $ONOO^-$, that contribute to microbial inactivation and surface modification.

169 Fig. 3 (b) shows that ozone (O_3) was generated during the DFD plasma treatment time. DFD plasma generated
170 approximately 0.5 ppm of ozone during the treatment of aerosolized pathogens, whereas the concentration
171 increased to 6–7 ppm when treating filter-attached pathogens. After the plasma was turned off, the ozone level
172 returned to zero within 1 min. In this experiment, it is presumed that the ozone generated during the nebulization
173 of the bacterial suspension to produce aerosols was vented out by the operation of the pump. In contrast, when the
174 DFD plasma was applied to the filter-attached pathogens, the pump was turned off, which likely increased the
175 ozone concentration.

176

177 **Experiment I: Bactericidal Effects of DFD Plasma on Aerosolized, Filter-Attached, and Overall Pathogens**

178 Fig. 4 shows the bacterial inactivation of aerosolized, filter-attached, and overall pathogens treated with DFD
179 plasma. When the bacterial suspension was nebulized to generate aerosols without DFD plasma treatment
180 (control), the surviving populations of *B. thuringiensis*, *S. marcescens*, and *E. coli* O157:H7 were approximately

181 4.57, 6.19, and 5.04 Log CFU/cm², respectively. The populations of *B. thuringiensis*, *S. marcescens*, and *E. coli*
182 O157:H7 in the aerosolized pathogens treated with DFD plasma did not differ significantly from those in the
183 control group. The *B. thuringiensis* population was significantly decreased by 1.20 Log CFU/cm² compared with
184 those in the control when the filter-attached pathogens were treated with DFD plasma, whereas the *S. marcescens*
185 and *E. coli* O157:H7 populations were not significantly decreased compared with those in the control. However,
186 when DFD plasma was continuously applied to both aerosolized and filter-attached pathogens (overall pathogens),
187 the populations of *B. thuringiensis*, *S. marcescens*, and *E. coli* O157:H7 were significantly reduced by 1.24, 1.05,
188 and 1.02 Log CFU/cm², respectively, compared with those in the control ($p < 0.05$).

189 In this study, aerosolized pathogens were generated by nebulizing a bacterial suspension, which remained
190 moisture-containing. Accordingly, we hypothesized that DFD plasma treatment of these aerosols would generate
191 RONS, thereby leading to effective bacterial inactivation. As confirmed by the optical emission spectroscopy
192 results, the DFD plasma generated various nitrogen radicals (Fig. 3 (a)) that could react with water molecules to
193 form additional RONS [16]. However, contrary to this expectation, bacterial inactivation was not observed under
194 the present experimental conditions. This finding contrasts with our previous study, in which 300 s (5 min) of
195 DFD plasma treatment during aerosolization of a SARS-CoV-2 suspension effectively inactivated 99.84% of the
196 viral population [10]. Given that viruses lack a cell wall, they are generally more susceptible to disinfection, and
197 the reactive species produced by the plasma can modify viral RNA, resulting in its inactivation [17]. Therefore,
198 even with the same plasma device, the antimicrobial efficacy of the treatment may vary depending on the
199 microorganisms' structural characteristics. Additionally, the ozone concentration generated by the DFD plasma
200 during treatment of aerosolized pathogens was approximately 0.5 ppm (Fig. 3 (b)), which might be too low to
201 achieve effective bacterial inactivation.

202 After nebulization, the aerosolized pathogens were attached to a PP filter located below the DFD plasma
203 generator by pump operation. Therefore, in this study, the inactivation effects of DFD plasma were evaluated on
204 pathogens attached to a filter. When filter-attached pathogens were treated with DFD plasma, a statistically
205 significant reduction was observed only for *B. thuringiensis* under the present experimental conditions. The
206 bactericidal effect of plasma is generally explained as being attributable to differences in the cell wall structures
207 of bacteria. Gram-positive bacteria possess a thick peptidoglycan layer, whereas gram-negative bacteria have a
208 thinner peptidoglycan layer and an additional outer membrane [15]. Given these structural differences, bacteria

209 often show varied responses to sterilization, including plasma treatment. In particular, Bende et al. [19] showed
210 that the outer membrane of gram-negative bacteria serves as a more effective barrier against RONS than the
211 peptidoglycan layer of gram-positive bacteria. Accordingly, several previous studies have suggested that gram-
212 positive bacteria are more susceptible to inactivation by plasma treatment [18,19]. However, in contrast to these
213 findings, some studies have reported opposing results, indicating that gram-negative bacteria may be more
214 sensitive because the thick peptidoglycan layer of gram-positive bacteria confers greater resistance to chemical
215 species [15]. Given the diverse results reported in previous studies, the present study could not clearly establish a
216 definitive distinction in plasma susceptibility between gram-positive and gram-negative bacteria.

217 As shown in Fig. 4, the populations of *S. marcescens* and *E. coli* O157:H7 did not differ significantly from
218 those in the control group, which may be attributed to the relatively low ozone concentration (approximately 6–7
219 ppm) generated during plasma treatment (Fig. 3 (b)). Supporting this, Gallagher et al. [20] reported that 28 ppm
220 of ozone produced by plasma could inactivate 97% of *E. coli* in aerosols, confirming the ozone-dependent
221 sterilization effect of plasma.

222 Interestingly, in the case of *S. marcescens* and *E. coli* O157:H7, no distinct bactericidal effects were observed
223 when the DFD plasma was individually applied to aerosolized or filter-attached pathogens. However, when both
224 steps were treated continuously (overall pathogens), a clearer bactericidal effect was observed, likely due to the
225 increased total plasma exposure time. In addition, plasma treatment of aerosolized pathogens may leave some
226 cells in a sub-lethally injured state, and these cells could become more susceptible to inactivation during the
227 subsequent plasma exposure applied to filter-attached pathogens [21]. By contrast, for *B. thuringiensis*, some cells
228 might already have been inactivated during the DFD treatment of filter-attached pathogens, which could explain
229 the absence of an additional bactericidal effect under continuous plasma treatment. However, whether these
230 mechanisms occurred in the present study remains uncertain and requires further verification.

231 In Experiment I, the DFD plasma treatment showed limited inactivation when applied individually to
232 aerosolized or filter-attached pathogens. By contrast, continuous treatment resulted in noticeable bacterial
233 reduction. However, since this effect was still limited, Experiment II was subsequently conducted to evaluate
234 whether the bactericidal effect could be enhanced by applying a storage time.

235

236 **Experiment II: Bactericidal Effect Depending on Storage Duration after DFD Plasma Treatment**

237 In Experiment I, the highest bactericidal effect was observed when both aerosolized and filter-attached
238 pathogens (overall pathogens) were continuously treated with DFD plasma. Therefore, these treatment conditions
239 were selected for Experiment II. In Experiment II, 0 and 1 min of storage time were applied after turning off the
240 DFD plasma to further enhance the bactericidal effect (Fig. 5).

241 The plasma device used in this study consists of a closed cylindrical chamber in which the inlet and outlet are
242 fitted with HEPA filters, thereby limiting the loss of reactive species. Under these conditions, reactive species can
243 remain even after the plasma is turned off, and these residual species are known to contribute to additional bacterial
244 inactivation. Leipold et al. [22] inoculated *Listeria innocua* onto glass slides, which were placed in polyethylene
245 bags and exposed to DBD plasma that was turned on and off. Ozone was preserved in a sealed bag for
246 approximately 10 min after exposure to DBD plasma for 30 s, thereby increasing the inactivation of the inoculated
247 *L. innocua*. Yong et al. [15] inoculated *E. coli*, *Salmonella* Typhimurium, and *Listeria monocytogenes* onto agar
248 plates and cheese slice samples. The samples were placed in plastic containers, exposed to DBD plasma, and left
249 for up to 5 min with DBD plasma turned off. The results showed that more bacteria could be inactivated as the
250 waiting time increased.

251 This study conducted a 1 min storage experiment to evaluate the bacterial inactivation capability of the residual
252 ozone after turning off the DFD plasma. As shown in Fig. 3 (b), residual ozone is still present for 1 min even after
253 the DFD plasma was turned off. Given that ozone is a representative reactive oxygen species with a relatively
254 long lifetime, we expected that it would contribute to an additional bactericidal effect [23]. However, as shown in
255 Fig. 5, no significant differences in bacterial inactivation were observed among the three species between 0 and 1
256 min of storage time. This can be attributed to the rapid decrease in the ozone concentration within 1 min of turning
257 off the DFD plasma, resulting in an insufficient level of bacterial inactivation (Fig. 3 (b)). Therefore, storage for
258 1 min in an environment with decreasing ozone did not have any noticeable bactericidal effects on the tested
259 bacteria.

260

261 **Experiment III: Bactericidal Effects of DFD Plasma According to the Treatment Time for Overall** 262 **Pathogens**

263 In Fig. 6, the effect of bacterial inactivation over time was shown by varying the DFD plasma discharge time
264 for filter-attached pathogens during the continuous treatment of aerosolized and filter-attached pathogens (overall

265 pathogens). The inactivation of all three bacterial species increased linearly with increasing plasma treatment time.
266 The population of *B. thuringiensis* was reduced by 1.24, 1.89, and 3.41 Log CFU/cm² at treatment times of 2, 5,
267 and 10 min, respectively. The population of *S. marcescens* decreased, with reductions of 1.05, 1.84, and 2.67 Log
268 CFU/cm² at 2, 5, and 10 min, respectively. Also, the population of *E. coli* O157:H7 decreased by 1.02, 1.81, and
269 2.94 Log CFU/cm² at the same treatment times, respectively. This implies that the bactericidal effect of DFD
270 plasma was significantly enhanced when the treatment time of filter-attached pathogens was increased after
271 applying DFD plasma to aerosolized pathogens for 2 min.

272 Concentration of aerosolized bacteria in indoor environments varies depending on environmental conditions,
273 seasonal changes, and human occupancy, but it generally remains within the range of approximately 2–3 Log
274 CFU/m³ [24]. As shown in Fig. 6, under the conditions showing the greatest bactericidal effect, the reduction level
275 ranged from approximately 2.6 to 3.4 Log CFU/cm². Thus, the DFD plasma treatment applied in this study was
276 expected to show an effective inactivation effect against aerosolized bacteria.

277 This study represents a preliminary investigation demonstrating the potential application of DFD plasma in
278 rearing environments such as edible insect cages. Therefore, this plasma device can be considered for installation
279 in insect-rearing cages and for operation with air circulation using a pump. However, further studies are required
280 to determine the practical applications of this device. In particular, since it is intended for use during the rearing
281 of edible insects, its potential adverse effects on insects must be thoroughly evaluated. Ozone, a key reactive
282 species in plasma sterilization [10], can inactivate aerosolized bacteria in rearing environments; however, its
283 potential adverse effects on edible insects must be carefully evaluated before practical application. Studies on the
284 effects of ozone on insects have shown that exposure to various combinations of ozone concentrations and
285 durations, such as 2–3 days at 5 ppm or 1 h at 1800 ppm, can lead to insect mortality [25]. Although the ozone
286 concentration used in the current study (approximately 7 ppm) did not cause insect mortality, further verification
287 is required. Additionally, technologies for the effective management and application of ozone emissions should
288 be developed, and the introduction of ozone catalysts should be considered to reduce ozone concentration [26].

289

290

Conclusions

291 This study evaluated the disinfection effects of DFD plasma on aerosolized pathogens associated with insect
292 pathogenic and foodborne bacteria that may occur in edible insect-rearing environments and confirmed its

293 potential applicability. The results showed that various RONS, including ozone, were generated during the DFD
294 plasma discharge. When DFD plasma was applied to aerosolized pathogens for 2 min or to filter-attached
295 pathogens for 2 min, no bactericidal effects were observed. However, a significant inactivation effect was
296 observed when both aerosolized and filter-attached pathogens were continuously treated with DFD plasma.
297 Especially, the highest bactericidal effect was obtained when DFD plasma was applied to aerosolized pathogens
298 for 2 min, followed by an additional 10 min of treatment with filter-attached pathogens. In this treatment,
299 reductions of 3.41, 2.67, and 2.94 Log CFU/cm² were observed in *B. thuringiensis*, *S. marcescens*, and *E. coli*
300 O157:H7, respectively.

301 Inactivation of aerosolized microorganisms in edible insect rearing environments is expected to play an
302 important role in ensuring the productivity and safety of edible insect production. This approach may also
303 contribute to reducing microbial contamination risks and improving hygiene management in insect-rearing
304 systems. However, given that this study was conducted under simulated conditions, further validation is required
305 to confirm whether similar effects can be achieved in actual insect-rearing systems.

306

307 **Competing Interests**

308 The authors declare that they have no known competing financial interests or personal relationships that could
309 have appeared to influence the work reported in this paper.

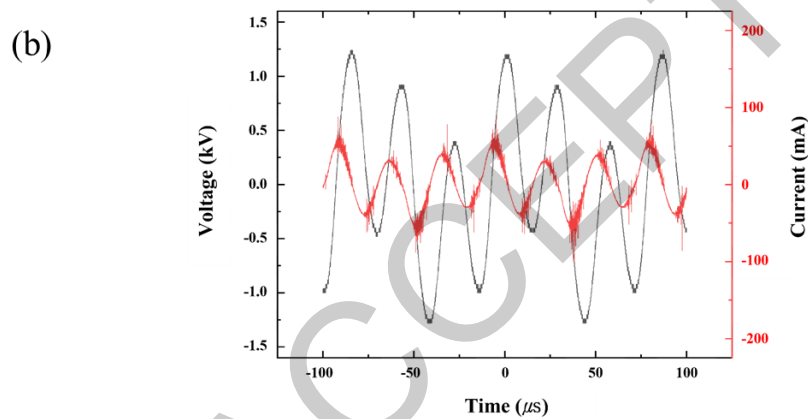
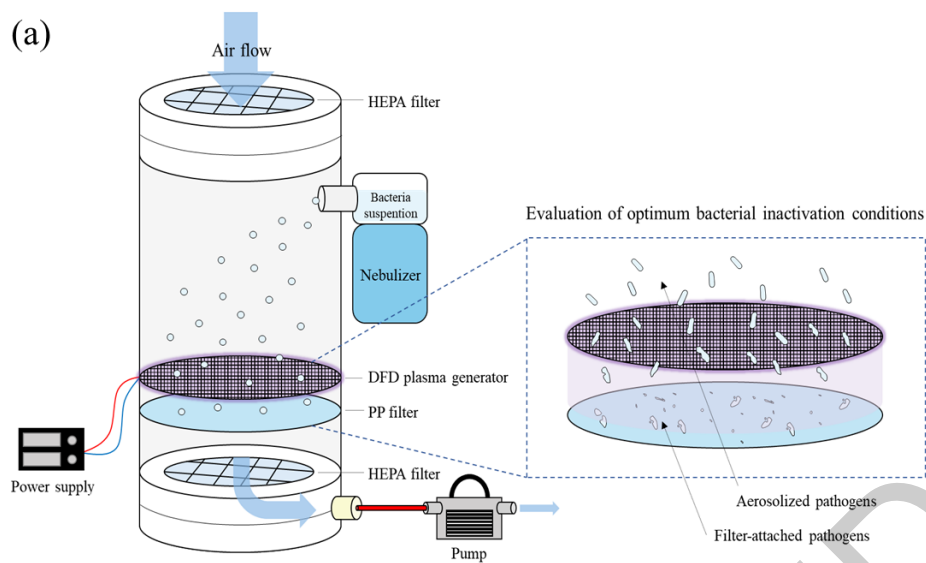
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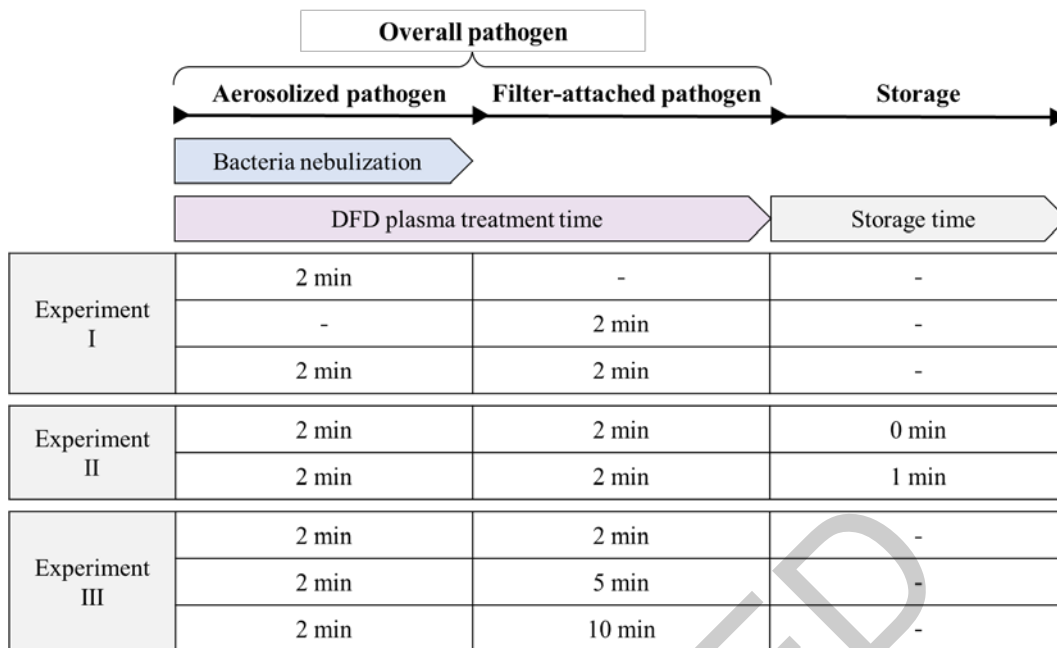
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 386 **Fig. 1.** (a) Schematic diagram of the dielectric filter discharge (DFD) plasma system for aerosolized
 387 pathogen inactivation and (b) voltage and current waveforms during plasma treatment.

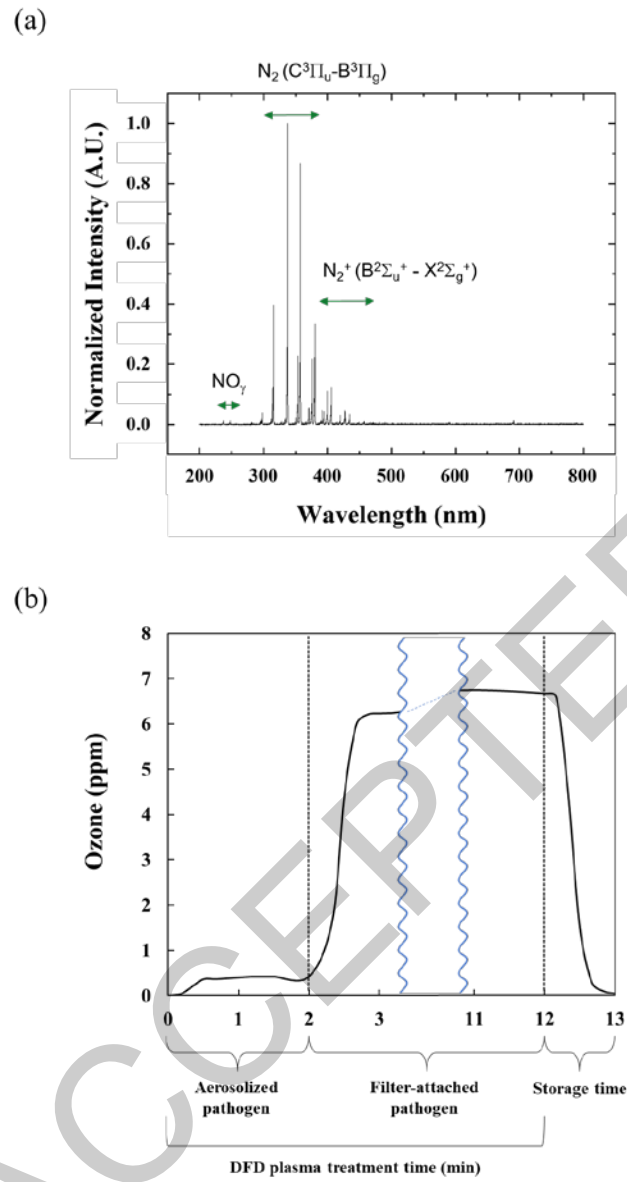
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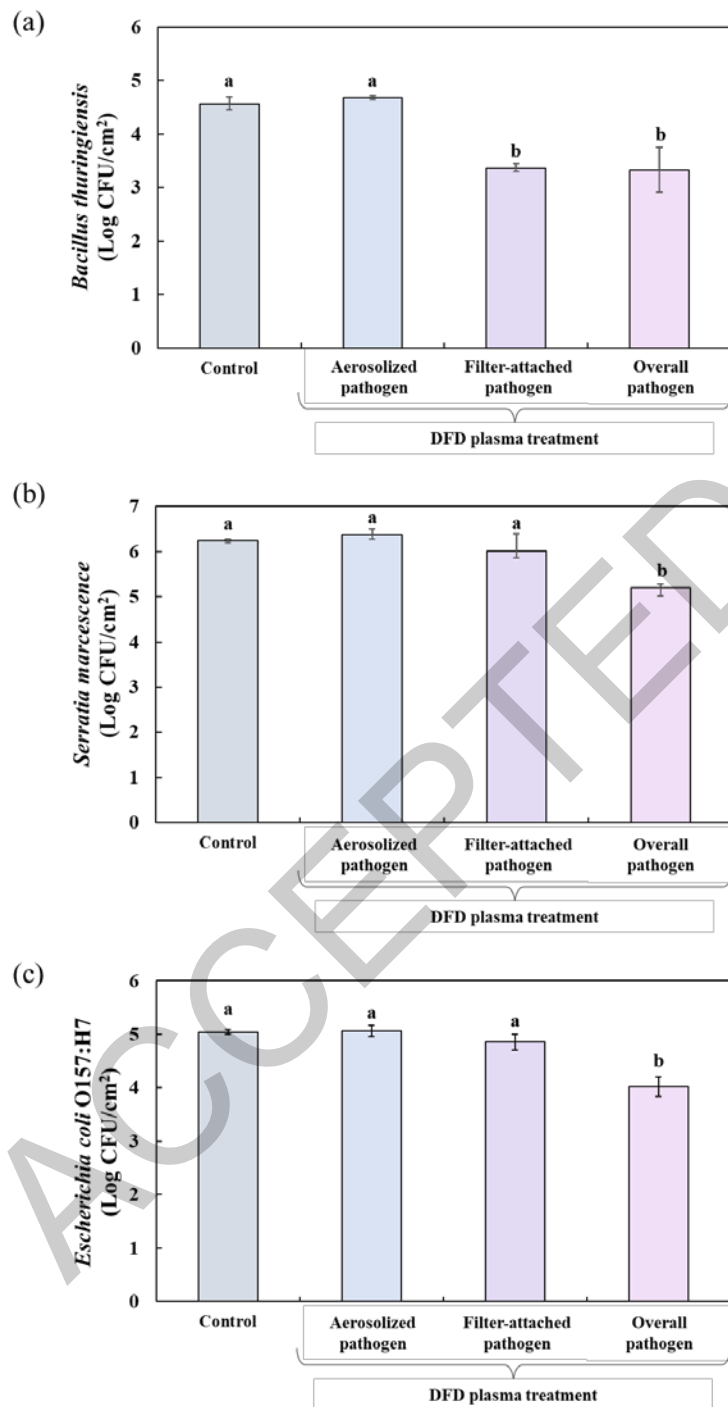
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Fig. 2. Diagram illustrating the DFD plasma treatment process in this study.



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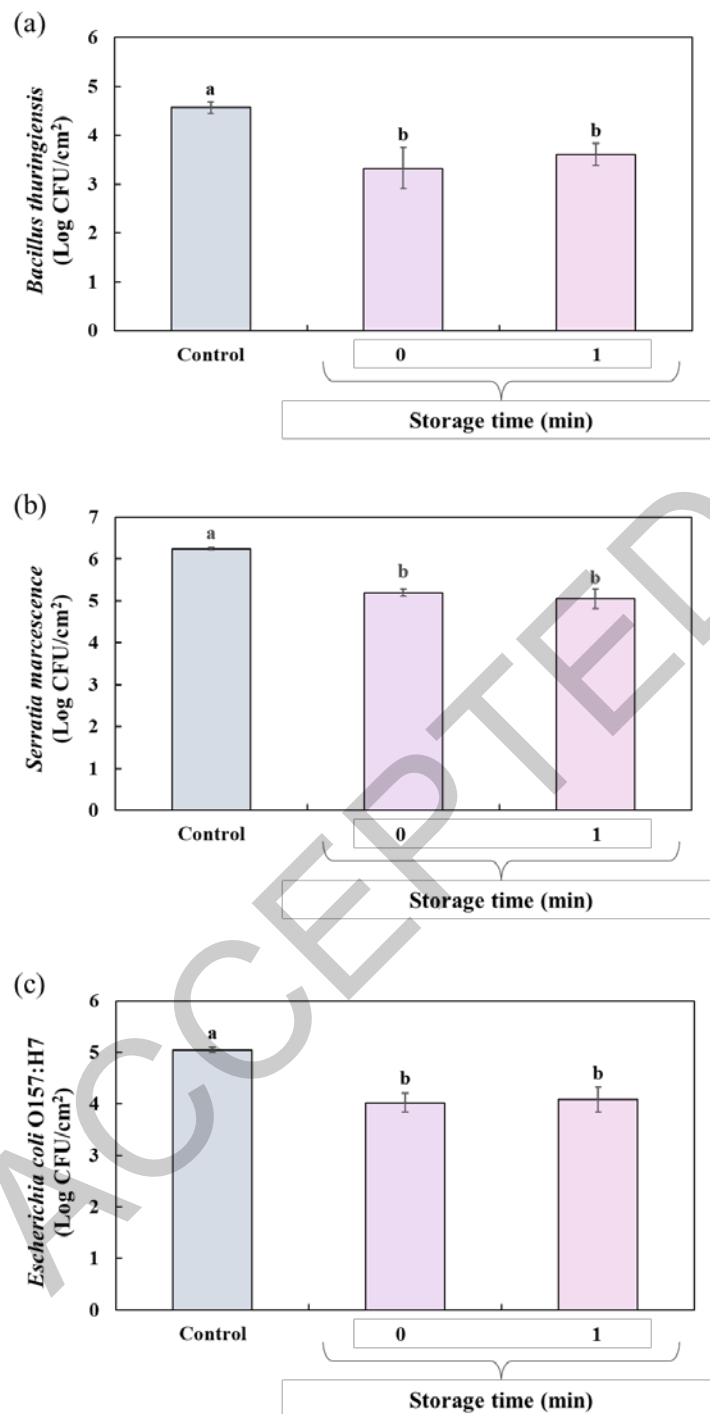
Fig. 3 (a) Optical emission spectrum and (b) ozone concentration during DFD plasma treatment.



393

394 **Fig. 4.** Experiment I: Inactivation effect of DBD plasma treatment on aerosolized pathogens (2
 395 min), filter-attached pathogens (2 min), and both overall pathogens (aerosolized + filter-
 396 attached, each for 2 min). (a) *Bacillus thuringiensis*; (b) *Serratia marcescens*; and (c)
 397 *Escherichia coli* O157:H7.

398 ^{a,b}The means with different letters are significantly different ($p < 0.05$).

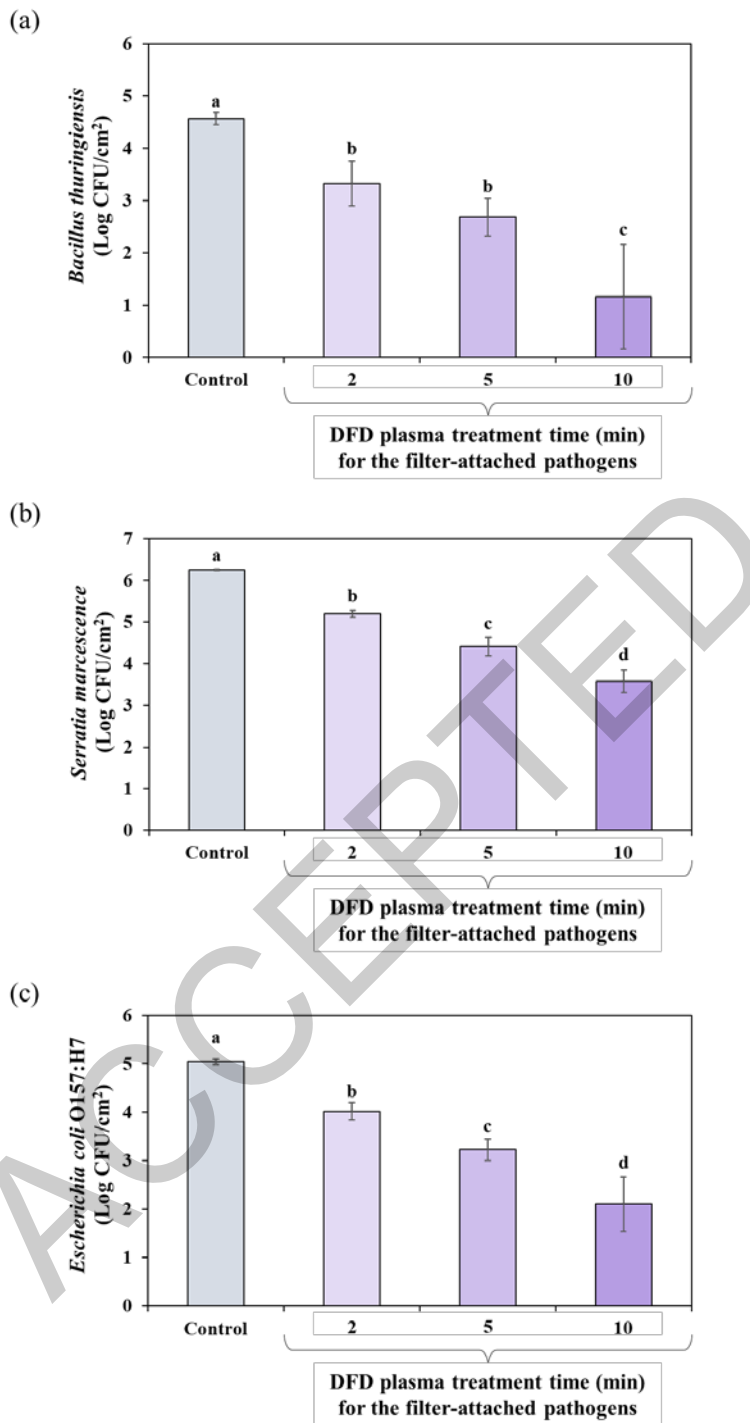


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400 **Fig. 5.** Experiment II: Inactivation effect on overall pathogens with different storage times (0
 401 and 1 min) after DFD plasma treatment (a) *Bacillus thuringiensis*; (b) *Serratia marcescens*;
 402 and (c) *Escherichia coli* O157:H7.

403 ^{a,b}The means with different letters are significantly different ($p < 0.05$).

404



405
 406 **Fig. 6.** Experiment III: Inactivation effects of DFD plasma on filter-attached pathogens
 407 according to treatment time (2, 5, and 10 min) after continuous treatment of aerosolized
 408 pathogens (2 min) (a) *Bacillus thuringiensis*; (b) *Serratia marcescens*; and (c) *Escherichia coli*
 409 O157:H7.

410 ^{a-d}The means with different letters are significantly different ($p < 0.05$).